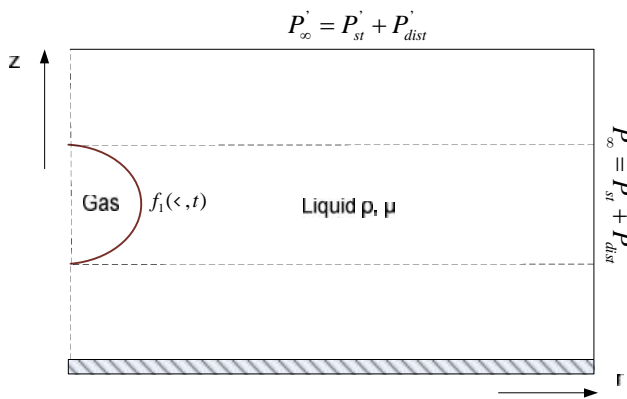


(Zhao et al. 2005; Vos et al. 2008).
 Liu et al. (2011)
 Mooney-Rivlin
 Navier-Stokes
 Tsiglifis and Pelekasis (2013)
 (Tsiglifis and Pelekasis 2011).
 contrast agents (Qin and Ferrara 2006)
 (Sassaroli and Hynynen 2005)

2.

R_0
 (μ 1).



μ 1: μ μ μ .

Navier-Stokes,

$$\frac{\partial \mathbf{u}}{\partial t} + (\mathbf{u} \cdot \nabla) \mathbf{u} = -\nabla p + \frac{1}{Re} \nabla^2 \mathbf{u}, \quad \nabla p = -p \mathbf{I} + \frac{1}{Re} \nabla^2 \mathbf{u} \tag{1}$$

$$\nabla \cdot \mathbf{u} = 0 \tag{2}$$

Re = ... $\tilde{S}_f R_0^2 / \nu$ Reynolds

$$\left(-p \mathbf{I} + \frac{1}{Re} \nabla^2 \right) \cdot \mathbf{n} + P_G \mathbf{n} = \frac{(\ddot{\mathbf{e}}_s \cdot \mathbf{n}) \mathbf{n}}{We} + \mathbf{F} = \frac{2k_m \mathbf{n}}{We} + \mathbf{F} \tag{3}$$

\mathbf{n} , P_G , $\ddot{\mathbf{e}}_s, k_m$, We Weber

$$\mathbf{F} = \left[k_s \dot{r}_s + k_w \dot{r}_w - \frac{1}{r_0} \frac{\partial}{\partial S} (r_0 q) \right] \mathbf{n} - \left[\frac{\partial \dot{r}_s}{\partial S} + \frac{1}{r_0} \frac{\partial r_0}{\partial S} (\dot{r}_s - \dot{r}_w) + k_s q \right] \mathbf{e}_s \quad (4)$$

$r_0 = r.$

(Timoshenko & Woinowsky 1959; Pozrikidis 2001):

$$q = \frac{1}{r_0} \frac{\partial r_0}{\partial S} \left[\frac{\partial}{\partial r_0} (r_0 m_s) - m_w \right] \quad (5)$$

Mooney-Rivlin, Tsigklifis & Pelekasis (2008, 2011, 2013) Vlachomitrou & Pelekasis (2017).

$$\mathbf{u} = \frac{D\mathbf{r}_s}{Dt} \quad (6)$$

$$P_G(t=0) = P_{st} + \frac{2}{We} \quad (7)$$

Young-Laplace:

$$P_G(t=0) V_G^*(t=0) = P_G(t) V_G^*(t) \quad (8)$$

$V_G(t=0) = 4f / 3$

μ 1.07.

3.

Lagrange splines, Lagrange splines, Euler. (Christodoulou & Scriven, 1992 ; Tsiveriotis & Brown 1992 ; Dimakopoulos & Tsamopoulos 2003)

Bjerknes (μ^2).

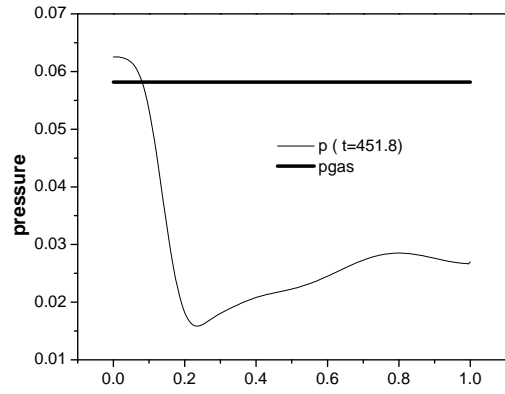
(prolate μ^2).

(μ^3).

Bjerknes μ .

(oblate μ).

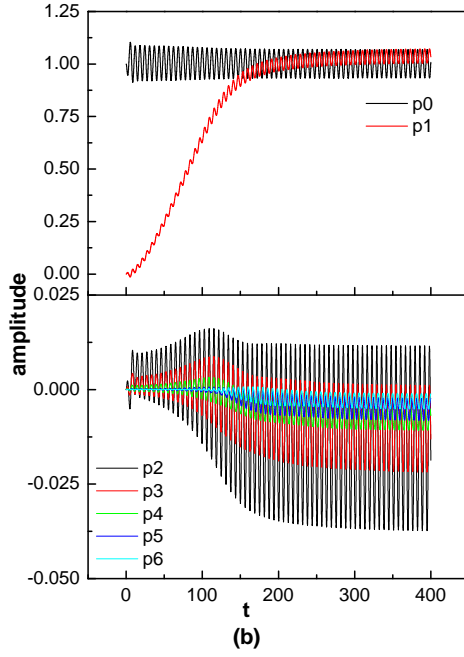
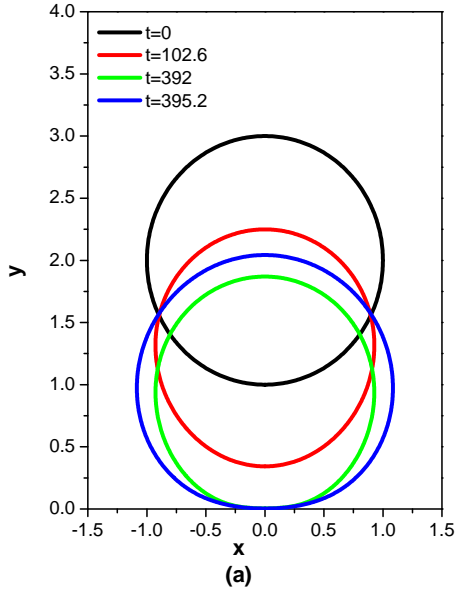
2).



μ^3 : $f=1.7\text{MHz}$ $=2$.

Bjerknes μ .

(μ^4 5).

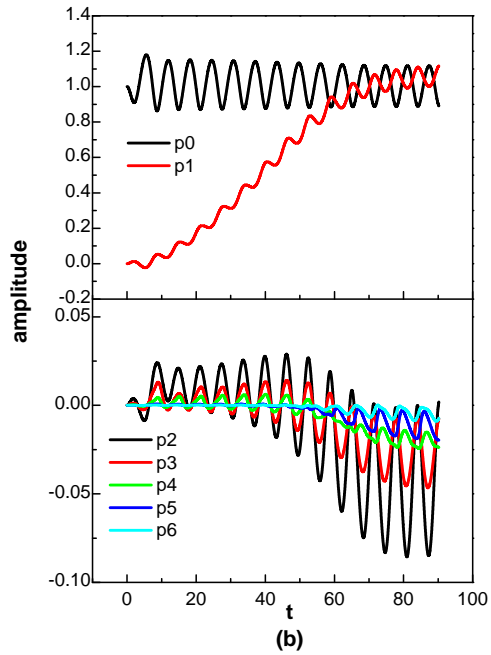
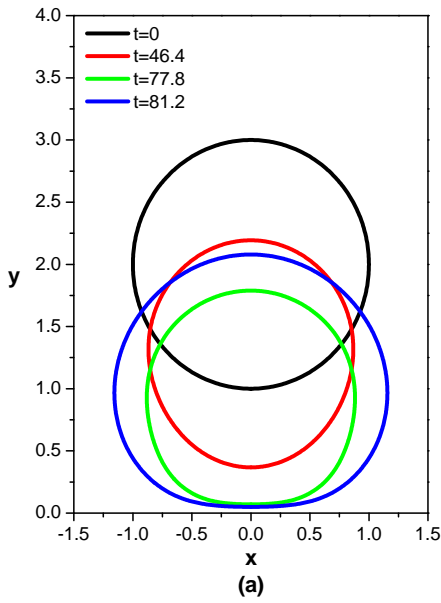


μ 4: ()

μ , ()

$f=1.7\text{MHz}$

$\mu = 1.$



μ 5: ()

μ , ()

$f=1.7\text{MHz}$

$\mu = 1.7.$

μ , μ

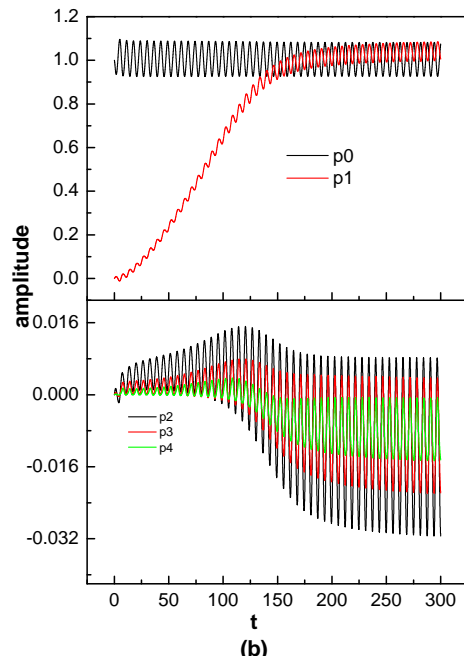
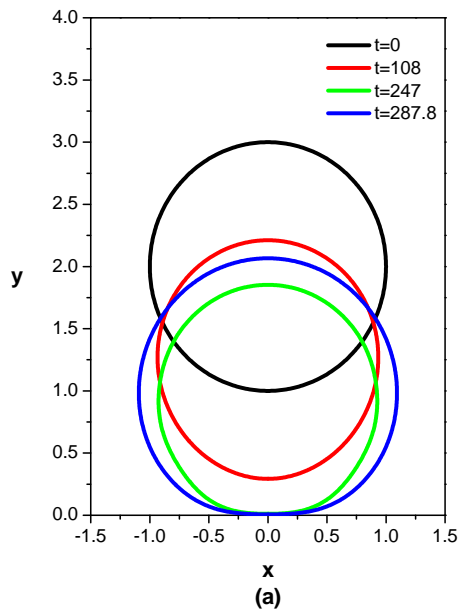
(μ 6 , 7).

μ μ μ

μ , μ ,

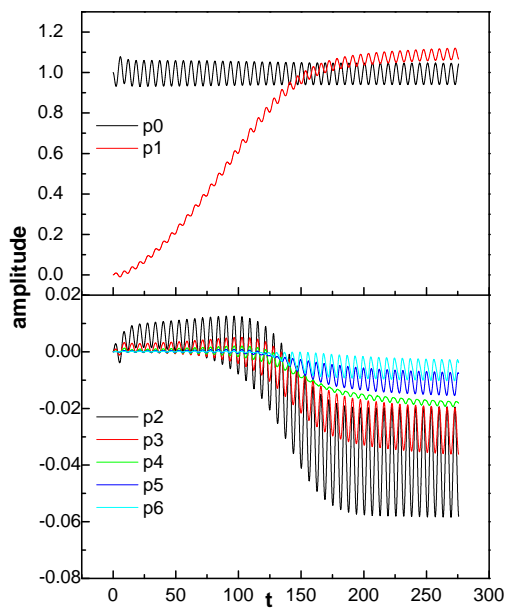
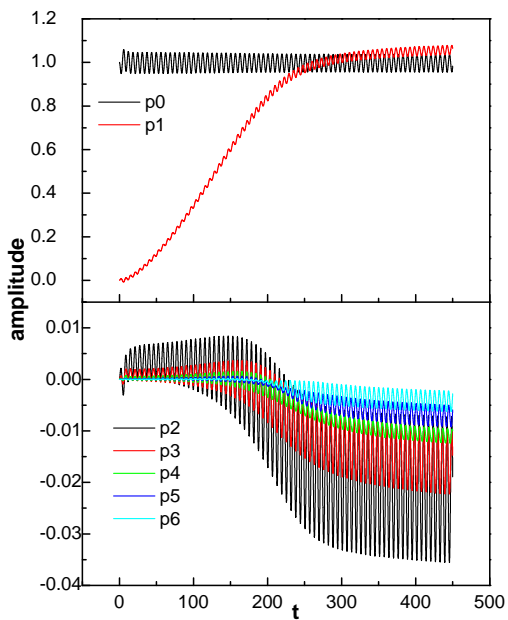
μ jet, μ

(μ 7)



μ 8: ()
 μ
 300×10^{-9} g/s.

μ , ()
 $f=1.7\text{MHz}$, $\mu=3$, $\mu \mu$



μ 9:
 $f=3.4\text{MHz}$, μ () =3 () =4.

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NUMERICAL STUDY OF THE TRAPPING OF AN ENCAPSULATED MICROBUBBLE ON A RIGID WALL

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ABSTRACT

The dynamic behavior of encapsulated microbubbles plays a key role in many biomedical applications among which the most important are medical imaging of vital organs and targeted drug delivery. In the present study the Finite Element Methodology is used to examine the dynamic response of an elastic microbubble to acoustic disturbances in a wall restricted flow. Emphasis is given on determining the mechanism and defining the conditions that enable the trapping of the bubble on the wall. It was found that the microbubble performs volume pulsations and moves towards the wall due to the secondary Bjerknes forces, whereas as it approaches closer to the wall the liquid starts to resist its movement with a local increase in the pressure (lubrication pressure) near the north pole. For a microbubble with given viscoelastic shell properties and for a given frequency of external disturbance these two opposing forces balance each other as long as the acoustic amplitude is smaller than the critical threshold for parametric mode excitation that stability analysis predicts. In this case the microbubble is eventually trapped on the wall where it continues to oscillate with its shape becoming flat on the lower pole. For greater acoustic disturbances buckling occurs on the north pole without jet formation as shell viscosity absorbs energy and moreover the shell resists to bending. Finally, it was found that by increasing shell viscosity or the external frequency the trapping procedure is facilitated.